Essential roles of noise in neural coding and in studies of neural coding

Edwin R. Lewis a,*, Kenneth R. Henry b, Walter M. Yamada c

a Department of EECS, University of California, Berkeley, CA 94720-1770, USA
b Department of Psychology, University of California, Davis, CA 95616, USA
c Department of Physiological Science, University of California, Los Angeles, CA 90095, USA

Abstract

We present examples of results from our studies of auditory primary afferent nerve fibers and populations of such fibers in the frog and gerbil. We take advantage of the natural dithering effect of internal noise, where it is sufficient, to construct highly predictive descriptive models (based on the Wiener series with kernels derived from white-noise analysis). Where the internal noise is insufficient, we enhance dithering by applying external acoustic noise together with our stimuli. Using acoustic noise as a background sound, orthogonal to the stimulus waveform, we show that under some circumstances such background sound can enhance the ability of individual fibers and populations of fibers to encode the stimulus waveform. © 2000 Elsevier Science Ireland Ltd. All rights reserved.

Keywords: Wiener series; Dithering with noise; Auditory spectrotemporal filters; Coding in auditory afferents

1. Introduction

In his theoretical studies of action potentials, FitzHugh (1955, 1961) concluded that the underlying dynamics were represented well by a state-plane divided by a single line segment (a separatrix) into two regions. In one of the two regions, all trajectories corresponded to full amplitude spikes; all trajectories originating in the other region corresponded to graded responses. The resting state of the system was represented by a stable point in the graded-response region. All trajectories, both full-spike and graded-response, converged on that point. Thus, full-spike trajectories eventually carried the system back into the region of graded responses. This required that the full-spike region and the graded-response region merge, beyond the end of the separatrix. A brief stimulus that moved the state of the system from the resting state to any point on the near side of the separatrix produced a graded response; one that moved the state of the system to any point on the far side of the separatrix produced a full spike. For both classes of trajectory, the closer the trajectory was to the separatrix, the farther along the separatrix the trajectory coursed before diverging away from it. Thus, FitzHugh’s state-plane model described a system capable of graded responses

* Corresponding author. Tel.: +1-510-6426954; fax: +1-510-6438426.
E-mail address: lewis@eecs.berkeley.edu (E.R. Lewis).
with amplitudes ranging from zero to that of a full spike.

A commonly-cited feature of action potentials in real neurons, however, is the all-or-none (threshold) property. The amplitudes of graded responses at spike triggers usually are limited to values very much less than the amplitude of a full spike. Responses with intermediate amplitudes usually are not seen.

In the region of the state plane reachable from the resting state by means of brief stimuli, both classes of trajectories (full spike and graded response) diverged strongly from the separatrix. This divergence gradually became weaker toward the far end of the separatrix, but it remained strong well along the way. Thus, where they could be reached by brief stimuli, the trajectories close to the separatrix were concentrated on a state-plane structure very much like a knife-edge ridge. A tiny nudge to one side or the other would move the state of the system off of the ridge and onto a trajectory moving rapidly away, toward a full spike or toward the resting point. FitzHugh concluded that the noise in the real system (but not included explicitly in the state-plane model) would provide such nudges and would thus make it virtually impossible for the system to remain long on the knife-edge ridge. Thus, the presence of noise would create what FitzHugh called a "no-man’s land," a large area into which the system was denied entry by the presence of noise. Because all trajectories corresponding to graded responses of intermediate or large amplitude passed through this area, such responses were not available. Thus, FitzHugh concluded that the spike trigger owes its all-or-none (threshold) property to the presence of noise.

Attacking this problem quantitatively with the state-plane model, Clay (1976) reached the same
conclusion as FitzHugh, but he also showed that the amplitudes available to the graded responses should increase conspicuously as the speed of the channel kinetics involved in spike triggering increased. If the state of the system could move more rapidly along the knife edge ridge, its chances of being nudged off of the ridge were reduced. Furthermore, the farther it was able to move along the ridge, the less steep were the ridge edges it faced, making further motion along the ridge more probable. One way to increase the speed of channel kinetics is to increase temperature. Cole et al. (1970) in fact had already shown that the all-or-none spike property of the squid giant axon gives way to completely graded response (all amplitudes between zero and full-spike amplitude are available) when the axon is warmed about 20°C above its normal temperature. This increased the channel kinetics by about an order of magnitude, evidently without increasing the noise amplitude enough to compensate. All of this suggests that FitzHugh was correct, the spike trigger does owe its threshold properties to the presence of noise.

At nearly the same time that FitzHugh was drawing his conclusions, Lowenstein (1956) was asserting that with respect to external sensory input, randomly firing, spontaneously-active primary sensory neurons have no threshold. In other words, he was asserting that the response of a primary sensory axon (a change in the instantaneous spike rate) to an arbitrarily weak sensory input could be observed if one applied the stimulus repeatedly and had the patience to wait for the averaged response to emerge from the noisy background spike rate. This notion subsequently was explored quantitatively by Stein and coworkers (Stein, 1970; French and Stein, 1970), and later by others, including our laboratories (e.g. Yu and Lewis, 1989). The conclusion reached by all is the following: independent noise at the spike trigger of each member of a population of axons can counteract the effects of threshold (the all-or-none property) and allow the population to encode continuous input signals in a continuous manner, to signal levels well below the threshold of the individual spike trigger. This was essentially Lowenstein’s conclusion as well. It is analogous to dithering, which is employed by engineers to soften the effects of the lowest-level bit in digitally recorded waveforms (Vanderkooy and Lipshitz, 1984). In dithering (which relies on a very high sampling rate in a single channel rather than on a large number of parallel channels), added noise makes the system responsive to signal amplitudes that otherwise would be below the threshold for that lowest-level bit. The process also has appeared in the literature as the essential ingredient in a phenomenon labeled “stochastic resonance” (Wiesenfeld and Moss, 1995).

One can summarize all of these results as follows: regarding threshold, noise giveth and noise taketh away. It is the taking away part that has been especially interesting to people in the field (hearing research) of the three authors of this paper.

2. Making the spike trigger invisible

The temporal coding of complex acoustic waveforms by peripheral auditory nerve fibers (individually and collectively) has been a central theme of many investigations (e.g. Young and Sachs, 1979; Bodnar and Capranica, 1994). Probably because frogs are known to be especially responsive to the temporal aspects of acoustic stimuli, most such studies in recent years have been focussed on those animals. A major goal of these studies has been the derivation of a descriptive model of the primary auditory unit (afferent axon along with its peripheral tuning structures) that can predict the temporal patterns of its responses to acoustic waveforms of arbitrary complexity (e.g. Lim, 1990; Kumerasen et al., 1996).

Under typical experimental conditions, frog auditory units usually have very low spontaneous spike rates, and they typically produce only a few extra spikes in response to a single presentation of a stimulus waveform. In most such frog units, when the waveform is presented repeatedly those few spikes occur repeatedly at very nearly the same times relative to the waveform. This is reminiscent of the results of studies with spike-trigger
models (French and Stein, 1970; Yu and Lewis, 1989). When a stimulus waveform is applied repeatedly to an undithered spike-trigger model, the spikes occur at precisely the same place in the stimulus cycle each time the stimulus is presented. The timing is determined by the particulars of the spike-trigger model (e.g., dynamics of accommodation and refractoriness). Thus, evidently, in most frog auditory units, the timing of spikes in response to an acoustic stimulus waveform depends on the particulars of the spike trigger as much as it does on the properties of the peripheral tuning structure. This seems to have made predictive modeling very difficult for these units. To date, nobody has succeeded in creating a model that will predict the temporal responses of such a unit to a waveform of arbitrary shape.

In mammalian auditory units and in a few frog auditory units, including all of those with substantial background spike activity, the temporal patterns of spike responses tend to vary conspicuously and randomly from one presentation of a stimulus waveform to the next. This implies the presence of noise sources, within the ear, that impose randomness (dithering) on the responses to the stimulus waveform. In such cases, prediction with a model is limited to response statistics. The statistic employed most widely by hearing researchers is the average temporal pattern of spikes, or peristimulus time histogram (PSTH), taken over many presentations of the stimulus waveform. Each PSTH bin represents a segment of time whose duration is equal to the unit of temporal resolution (the bin sampling time during each stimulus presentation), which is an indivisible instant of time in the histogram’s discrete-time presentation of the data. Division of the total spike count in a bin by the total time represented by that bin (bin sampling time during each stimulus presentation times the number of presentations used to construct the PSTH) yields the instantaneous spike rate for the corresponding time in the stimulus cycle. Thus, the PSTH yields a discrete-time estimate of the temporal pattern of the modulation of spike rate, instant by instant, through the time course of the stimulus waveform. When the dithering imposed by the internal noise of the ear is sufficient, this temporal
Fig. 3. Responses of a gerbil cochlear unit (Lewis and Henry, 1995) to a probe stimulus (a 73-dB (SPL), 700-Hz tone burst). The unit was tuned to 8 kHz, where its threshold was 34 dB SPL. The upper PSTH shows the smoothed response to 260 presentations of the probe stimulus alone; the unit clearly responded to the abrupt onsets and offsets of the tone burst. The lower PSTH shows the smoothed response to 840 presentations of the same probe stimulus together with a 51-dB (SPL) noise burst of the same duration. The noise bandwidth was 9.7 kHz. In the presence of the noise-burst, the probe elicited an unclipped sinusoidal modulation of instantaneous spike rate strongly phase-locked to the 700 Hz tone.

Fig. 4. The left-hand panel shows the extracellular voltage taken over approximately the first two millimeters of the cochlear nerve of the gerbil, averaged over approximately 500 repetitions of a near-threshold (13-dB SPL) probe stimulus. The stimulus comprised two frequency components (10.00 and 10.93 kHz) of equal amplitude. The adjacent right-hand panels show the corresponding amplitude spectra (from discrete Fourier transform). The 930-Hz sinusoidal component of the voltage has been shown to be the consequence of the summed sodium currents from all of the spiking zones (nodes of Ranvier) along the two-millimeter nerve segment (Henry, 1995). It thus corresponds to a 930-Hz modulation of instantaneous spike rate over a population of units tuned to the neighborhood of the probe-stimulus frequency (10–11 kHz). Cochlear units are unable to respond linearly at frequencies as high as 10 kHz. Like high frequency frog units, however, they are presumed to produce a component of instantaneous spike rate that is proportional to the square of the (positive) envelope of the linearly filtered stimulus waveform. In this case, that would be a distorted 930-Hz sinusoid. The top waveform in the figure contains the response to the probe stimulus alone. The middle waveform contains the response to the probe stimulus plus a 10-ms noise burst (10 dB SPL, 300–17 000 Hz) added in the midst of the probe. The bottom waveform contains the response to the probe stimulus plus a 30-ms noise burst (also 10 dB SPL, 300–17 000 Hz). The 930-Hz component of instantaneous spike rate, taken over the entire population of cochlear-nerve axons, clearly was increased by the presence of the noise. This implies that the noise increased the number of units responding to the envelope of the filtered probe stimulus and/or increased the responsiveness of the units that already had been responding to the envelope of the filtered probe in the absence of the noise.

Fig. 4. The left-hand panel shows the extracellular voltage taken over approximately the first two millimeters of the cochlear nerve of the gerbil, averaged over approximately 500 repetitions of a near-threshold (13-dB SPL) probe stimulus. The stimulus comprised two frequency components (10.00 and 10.93 kHz) of equal amplitude. The adjacent right-hand panels show the corresponding amplitude spectra (from discrete Fourier transform). The 930-Hz sinusoidal component of the voltage has been shown to be the consequence of the summed sodium currents from all of the spiking zones (nodes of Ranvier) along the two-millimeter nerve segment (Henry, 1995). It thus corresponds to a 930-Hz modulation of instantaneous spike rate over a population of units tuned to the neighborhood of the probe-stimulus frequency (10–11 kHz). Cochlear units are unable to respond linearly at frequencies as high as 10 kHz. Like high frequency frog units, however, they are presumed to produce a component of instantaneous spike rate that is proportional to the square of the (positive) envelope of the linearly filtered stimulus waveform. In this case, that would be a distorted 930-Hz sinusoid. The top waveform in the figure contains the response to the probe stimulus alone. The middle waveform contains the response to the probe stimulus plus a 10-ms noise burst (10 dB SPL, 300–17 000 Hz) added in the midst of the probe. The bottom waveform contains the response to the probe stimulus plus a 30-ms noise burst (also 10 dB SPL, 300–17 000 Hz). The 930-Hz component of instantaneous spike rate, taken over the entire population of cochlear-nerve axons, clearly was increased by the presence of the noise. This implies that the noise increased the number of units responding to the envelope of the filtered probe stimulus and/or increased the responsiveness of the units that already had been responding to the envelope of the filtered probe in the absence of the noise.
3. Making peripheral axons more sensitive to pure sine waves

The inspiration for Lowenstein’s conclusions regarding the effects of dithering came largely from experiments in which simple stimuli, such as velocity ramps and sinusoids, were employed. The effects are especially clear with sinusoids. These have been applied widely in physiological studies of acoustic sensors and sensors of head orientation and motion. When the frequency of such a stimulus is sufficiently low (less than about 4 kHz in mammals, less than about 800 Hz in amphibians, reptiles and fish), the instantaneous spike rate of an inner-ear axon responsive to that frequency will show a component that is modulated at that frequency and very easy to detect (by phase-locked analysis). If the sinusoidal stimulus is sufficiently small and there is a sufficiently large background component of firing (i.e. a sufficiently large d.c. component of instantaneous spike rate), then the modulation can be very close to linear. Sufficiency for the d.c. spike rate component in that case is slightly greater than half of the peak-to-peak linear amplitude of the nearly linear modulation. As a consequence of the circuit-theory metamodel and the extensive body of knowledge associated with it (e.g. Lewis, 1996), nearly linear dynamics are richly interpretable in terms of underlying biophysics. Thus, where they lead to such dynamics, sinusoids are excellent probe stimuli.

For gerbil cochlear units, a small-amplitude sinusoidal stimulus was used as probe to measure the changes in inner-ear auditory sensitivity in response to changes in ambient sound levels. The background sound was band-limited white noise. Sudden increases in the amplitude of that noise typically produced sudden transient increases in the linear responsiveness of the system to the probe stimulus (Lewis and Henry, 1995). The most conspicuous examples occurred in units tuned to high frequencies (e.g. the unit in Fig. 3). The noise was turned off and on and the axons exhibited no linear response at all to a low-frequency probe sinusoid when the noise was off. When the noise was on, the probe produced close to 100% sinusoidal modulation of instantaneous spike rate. Thus, axons that were unresponsive to the probe in the absence of background sound became very responsive when that sound was added. This means that adding the background sound (a noise signal in this case) increased the population of axons in the auditory nerve that responded to the probe stimulus. Whole-nerve measurements (Fig. 4) strongly support this conclusion.

4. Uncited reference

Yamada et al. (1996)

Acknowledgements

Research supported by Grant DC00112 from the National Institute of Deafness and Communicative Disorders. We thank Eva Hecht Poinar for help with the illustrations.

References


